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Description

This invention relates to sensors for use in biological, biochemical and chemical testing and in particular to immunosensors used to monitor the interaction of antibodies with their corresponding antigens.

When antibodies are immobilised on a surface, the properties of the surface change when a solution containing a corresponding antigen is brought into contact with the surface to thus allow the antigen to bind with the antibody. In particular, the change in the optical properties of the surface can be monitored with suitable apparatus.

The phenomenon of surface plasmon resonance (SPR) can be used to detect minute changes in the refractive index of the surface as the reaction between the antigen and the antibody proceeds. Surface plasmon resonance is the oscillation of the plasma of free electrons which exists at a metal boundary. These oscillations are affected by the refractive index of the material adjacent the metal surface and it is this that forms the basis of the sensor mechanism. Surface plasmon resonance may be achieved by using the evanescent wave which is generated when a p-polarised light beam is totally internally reflected at the boundary of a medium, e.g. glass, which has a high dielectric constant. A paper describing the technique has been published under the title "Surface plasmon resonance for gas detection and biosensing" by Lieberg, Nylander and Lundstrom in *Sensors and Actuators*, Vol. 4, page 299. Illustrated in Figure 1 of the accompanying drawings is a diagram of the equipment described in this paper. A beam 1 of light is applied from a laser source (not shown) onto an internal surface 2 of a glass body 3. A detector (not shown) monitors the internally reflected beam 4. Applied to the external surface 2 of glass body 3 is a thin film 5 of metal, for example gold or silver, and applied to the film 5 is a further thin film 6 of organic material containing antibodies. A sample 7 containing antigen is brought into contact with the antibody film 6 to thus cause a reaction between the antigen and the antibody. If binding occurs the refractive index of the layer 6 will change owing to the size of the antibody molecules and this change can be detected and measured using the surface plasmon resonance technique, as will now be explained.

Surface plasmon resonance can be experimentally observed, in the arrangement of Figure 1, by varying the angle of the incident beam 1 and monitoring the intensity of the internally reflected beam 4. At a certain angle of incidence the parallel component of the light momentum will match with the dispersion for surface plasmons at the opposite surface 8 of the metal film. Provided that the thick-

ness of metal film 5 is chosen correctly there will be an electromagnetic coupling between the glass/metal interface at surface 2 and the metal/antibody interface at surface 8 as a result of surface plasmon resonance, and thus an attenuation in the reflected beam 4 at that particular angle of incidence. Thus, as the angle of incidence of beam 1 is varied, surface plasmon resonance is observed as a sharp dip in the intensity of the internally reflected beam 4 at a particular angle of incidence. The angle of incidence at which resonance occurs is affected by the refractive index of the material against the metal film 5 - i.e. the antibody layer 6 - and the angle of incidence corresponding to resonance is thus a direct measure of the state of the reaction between the antibody and their antigen. Increased sensitivity can be obtained by choosing an angle of incidence half way down the reflectance dip curve, where the response is substantially linear, at the beginning of the antibody/antigen reaction, and then maintaining that angle of incidence fixed and observing changes in the intensity of the reflected beam 4 with time.

Known systems of the type described with reference to Figure 1 utilise a prism as the glass body 3. A diagram showing this arrangement is given in Figure 2 which is simply an experimental set up intended to demonstrate surface plasmon resonance. The prism is shown under reference 8 and has applied to its undersurface a thin film 5 of metal. Light 1 from a laser source (not shown) is incident on the prism where it is refracted at point 9 before entering the prism. The internally reflected beam 4 is likewise refracted (at point 10) upon exiting from the prism.

One problem with the known SPR systems is the slowness of operation relative to changes in the refractive index of the antibody layer. Another problem, particularly related to the use of the prism shown in Figure 2, is that, as the angle of incidence is changed, either by moving the source, or rotating the prism, or both, the point on surface 2 at which the incoming beam is incident moves. Because of inevitable variations in the metal film 5 and the coating 6 of antibody, the angle of incidence which results in resonance changes as this movement occurs, which in turn introduces a further variable factor into the measurement and thus makes comparisons between the initial, unbound, state and the bound state of the antibody layer 6 less accurate.

According to the invention, there is provided a sensor for use in biological, biochemical or chemical testing, said sensor comprising a block of material transparent to electromagnetic radiation, a layer of metallic material applied to at least part of a first surface of said block, a layer of sensitive

material applied to the metallic layer, means for introducing onto the sensitive layer so as to react therewith a sample to be analysed, a source of electromagnetic radiation, said radiation being directed into said transparent block in such a way as to be internally reflected off said part of said surface, and detector means positioned to receive the internally reflected beam, said sensor being characterised by means for focussing said radiation onto said part of said surface in such a way that the incoming beam is a converging fan beam that spans a range of angles of incidence including that which causes surface plasmon resonance to occur and that said incoming beam gives a point or line of incidence on said first surface, the characteristics of which resonance is dependent upon the reaction between the sample and the sensitive layer, and wherein said detector means is operable to receive a range of angles within the span of the diverging fan beam resulting from the internal reflection of said incoming fan beam, which received range of angles is sufficient to enable said characteristics of the surface plasmon resonance to be detected.

Thus in the present invention, the speed of response is improved by providing that the incoming beam of radiation which is internally reflected at the glass/metal interface takes the form of a fan-shaped spread of electromagnetic radiation, usually in the visible or near-visible region. In this way, the progress of the resonant condition, as the reaction between the sample and the antibody layer proceeds, can be monitored. In one example, this can be achieved by taking a "solid" input beam from a source of electromagnetic radiation, and bringing it (the beam) to a focus at the point of incidence of the beam on the glass/metal interface. The input beam thus becomes equivalent to several beams incident upon the glass/metal interface over a range of angles. The equipment is chosen so that the range of angles spans the angle of dip corresponding to surface plasmon resonance together with a range of angles thereabout. The corresponding internally reflected beam is likewise effectively several beams and may be monitored by a large area detector, or by an array of angularly spaced detectors positioned to collect the whole emergent beam. Thus the detectors can encode the information from the whole of the dip within milliseconds. In this way, the progress of the resonant condition, as the reaction between the sample and the antibody layer proceeds, can be monitored.

The use of a fan shaped beam highlights the problems of the prism (see above) and, in order to avoid these, it is provided that the surface of the transparent, usually glass, body onto which the incoming light is incident is a curved, preferably circular, surface and is arranged, with respect to

the input beam of electromagnetic radiation, such that the beam enters orthogonally to the tangent to the surface at the point of entry. Preferably likewise that surface from which the internally reflected beam emerges is a curved, preferably circular, surface.

In a first embodiment of the invention, the transparent body takes the form of a glass hemisphere whose flat surface is covered with a thin metal film and a sensitive overlayer in the manner described above. The source of input electromagnetic radiation, for example a light source, is arranged so that the input beam enters the hemispherical body orthogonally to the tangent at the point of incidence, and thus the beam passes through unrefracted and is incident at the centre of the circular flat surface. The point of incidence on the flat surface is thus the same for all parts of the fan-shaped beam.

Shapes other than hemispherical can be used; for example hemicylindrical, which gives a line incidence, rather than a point, or truncated hemispherical or hemicylindrical in which the top is cut off - i.e. to form a body having two flat, probably parallel, surfaces with circular sides joining the surfaces.

The fan-shaped beam may be constrained to be substantially planar by being projected through a slit lying in a plane passing through the point of incidence and oriented vertically to that of the glass/metal interface. Alternatively, the expression "fan-shaped" may refer to a shape of a section of the input beam, and the beam itself may extend in other planes - for example wedge-shaped (giving a line of incidence), or conical shaped.

Although the layer applied to the metal film is described herein as an antibody layer for use in immunoassays, it will be seen that any sensitive layer whose refractive index changes upon an event occurring can be used to thus provide a sensitive detector having a wide variety of applications in the fields of biology, biochemistry and chemistry. As an example, the sensitive layer could be a DNA or RNA probe which would, during the test, bind with its complement in solution as represented by the sample to be tested.

The metal film material is commonly silver or gold, usually applied by evaporation. The film needs to be as uniform as possible in order to cater for minute movement in the point of incidence of the incoming beam. It is assumed that a structured metal film will give the best resonance and there are various ways in which the glass body can be pretreated to improve the performance of the metal film and in particular to control the natural tendency of such films to form discontinuous islands;

1. Immersion in molten metal nitrates and other molten salts. This has the effect of introducing ions into the surface in a manner which can be structured and which can act as foci for island formation.

2. Ion bombardment of cold or hot glass to introduce nucleating sites. The removal of the more mobile ions has been demonstrated to reduce the thickness at which the evaporated film becomes continuous.

3. Electroless plating or electroplating over lightly evaporated films (0 to 100 angstroms thick). Electroless plated films survive to a greater thickness than evaporated films and could form more stable nuclei for subsequent coating.

4. Evaporating on to electroless plated films. The electroless plated films have a stronger tendency to an island structure and to bigger islands with greater spacing than evaporating films. This could be of advantage in tuning to light of a prescribed wavelength.

Coating performance can also be improved by:

1. Controlling the glass surface temperature during coating. Using a higher temperature substrate increases the islands' size and the spacing between them and conversely.

2. Evaporating in the presence of a magnetic or electrostatic field or electron emission device to control the ion content of the vapour stream. The state of charge of the substrate is known to affect the island structure.

3. Controlling the angle of incidence of the evaporated vapour stream relative to the glass surface. The mobility of the evaporated atoms and hence their ability to form bigger islands is greater when the momentum of the atoms relative to the glass surface is increased.

In order that the invention may be better understood, some embodiments thereof will now be described by way of example only and with reference to the accompanying drawings in which:-

Figures 1 and 2 are diagrams of known experimental arrangements for demonstrating the surface plasmon resonance effect;

Figure 3 shows, in schematic outline, a cross-sectional view of a sensor in accordance with one example of the invention;

Figure 4 is a diagrammatic side view of another example of a sensor according to the present invention; and

Figures 5(a) and 5(b) illustrate the performance of which an arrangement in accordance with the invention is capable.

Referring now to Figure 3, a collimated beam 13 of electromagnetic radiation of width $2r$ from a source which is not shown but may conveniently comprise a laser diode collimator pen such as that manufactured under the model number TXCK 1200

by Telefunken Electronic, is incident upon a hemi-cylindrical focussing lens 14 of focal length f_1 , which causes the light to converge to a point 15 on an interface 27 between an optically transmissive component, generally shown at 28, and a reflective layer 19 in the form of a metallic coating. The optical component is, in this example, made up of a glass support plate or slide 16 (upon which the reflective layer is coated) and a hemi-cylindrical lens 11, with its centre of curvature located at the point 15. A suitable index matching fluid is provided, as shown at 29, between the facing surfaces of plate 16 and lens 11 and the arrangement is such that all light paths in the convergent beam which emerges from lens 14 travel radially of the optically transmissive component 28 and thus undergo no refraction and are focussed centrally on the point 15. A slit 30 constrains the convergent beam to a substantial planar fan shape, so that only a small area of reflective layer 19 is illuminated to reduce any effects due to non-uniformity of the metal coating.

The light internally reflected from point 15 travels as a divergent, planar, fan-shaped spread back out of the component 28 and is incident upon a focussing lens 31 which creates a light beam 32 which is substantially parallel-sided, or at least of reduced divergence compared to the fan-shaped spread of light emergent from component 28. Beam 32 is arranged to be incident upon a detector 18, for example an array of photo-sensitive detectors, and it will be appreciated that the main purpose of lens 31 is to reduce stray reflections in the array 18 ensuring that beam 32 is normal to its surface. If, however, the stray reflections are not of significance or if the array 18 can be conveniently placed close to the exit surface of component 28 (possibly even attached to or deposited on that surface) lens 31 is not required.

The array of detectors is arranged to generate electrical signals indicative of the variation of intensity of light with position across the beam 32; the SPR effect dictating that strong absorption will occur at a particular angle as determined by material in the fluid to which the reflective layer 19 is exposed. These electrical signals are sampled and digitised and fed to a suitable analysing arrangement which may include a microprocessor or larger computer.

It can be desirable, in the interests of minimising the disturbing effects of extraneous light without having to resort to the expense and inconvenience of shrouding the entire arrangement, or at least the components 5 and 28, to arrange that a characteristic modulation is impressed upon the light and that the detectors and/or the processing circuits are "tuned" to respond preferentially to such modulation.

A second embodiment of the invention will now be described by reference to Figure 4. Referring to Figure 4, the apparatus comprises a hemispherical body 11 made of transparent material such as glass or quartz housed within a casing 12. A source (not shown) of electromagnetic radiation produces a collimated input beam 13 of electromagnetic radiation. The frequency of the radiation must be such as to result in the generation of surface plasmon waves and in practice will be within or near the visible region. Suitable sources include a helium neon laser or an infra red diode laser, but an ordinary light source, with suitable filters and collimators, could be used.

A lens 14 is used to bring the parallel input beam 13 to a focus at a point 15 spaced just above the centre of the circular flat surface of the hemisphere 11. The point 15 lies in the surface of a slide 16 made of transparent material such as glass whose refractive index is equal or close to that of the hemisphere 11. The arrangement is such that the point 15 lies at the approximate centre of curvature of the curved surface of the hemisphere.

Radiation which is internally reflected at point 15 passes out of the hemisphere in the form of a divergent beam 17 and passes into a radiation sensitive detector 18 which gives an electrical output signal for analysis by external circuitry (not shown) in the manner described above. The detector may for example be a diode array, or a charge couple device or similar imaging device.

In a practical realisation of the apparatus, the metal film layer, shown under reference 19, is applied to the surface of the aforementioned slide 16. The point 15 to which the input beam is focussed thus lies on the interface between the metal film and the slide 16. Applied to the surface of the metal film is a sensitive layer 20 whose refractive index changes as the test progresses. The sensitive layer may for example be an antibody layer. The sensitive layer 20 is restricted to a relatively small active zone about the point 15 and within a central hole provided in a circular disc 21 of absorbent material. Overlying disc 21 are two further discs 22, 23 of non-absorbent material. A central aperture in upper disc 23 defines a well 25 into which a sample to be tested is placed. A central aperture 24 in disc 22 is of a size to cause liquid in well 25 to travel through by capillary action into the active zone above layer 20. The thickness of disc 21 is such as to define a depth for the active zone such as to promote radially outwards movement of the sample liquid emerging from aperture 24 by capillary action. The absorbent disc 21 absorbs sample which has flowed past the active zone.

The whole unit comprising slide 16, disc 21 and discs 22 and 23 is disposable so that a fresh unit, including sensitive layer 20 can be used for

each test. The slide 16 is placed upon the flat surface of the hemisphere 11, preferably after applying to the flat surface a thin layer of optical oil or grease to ensure good optical coupling between the hemisphere and the slide. Optionally, the hemisphere itself may be disposable, provided it can be produced cheaply enough, in which case there would be no need to include a separate slide 16, and the metal film 19 can be applied direct to the hemisphere.

In order to use the apparatus a sample to be tested, and containing an antigen capable of binding with the antibody molecules in layer 20, is placed in the well 25 and passes through aperture 24 by capillary action. Emerging from aperture 24, the liquid sample commences to flow radially outwards in all directions towards the absorbent disc 21, passing as it does so the antibody layer 20. The sample adjacent the layer 20 is thus being constantly replenished during the course of the test, which ensures maximum sensitivity.

As the sample flows past the layer 20 any antigen within the sample capable of binding with the antibody in layer 20 will do so, thus altering the refractive index of layer 20 as the reaction proceeds. This change in refractive index is continuously monitored during the test by directing at the point 15 the focussed light beam 13. Provided that conditions are correct - in particular the angle of incidence at the point 15 is correct - the application of beam 13 will result in the generation of a plasmon wave, thus extracting energy from the input beam and causing an attenuation in the intensity of the output beam 17 at a particular angle of incidence. The input beam is arranged such that the mid-angle of the range of angles of the input beam is approximately half-way down the reflectance dip, as described above, and the test is carried out at a constant angle of incidence, monitoring the intensity of the reflected beam above and below this mid point level. This gives a linear and highly sensitive output.

The initial reflectance dip which is chosen for setting up the angle of incidence should be the dip which results when some neutral or buffer solution is passed through the cell, or when the sample under test is passed through the cell but before any reaction thereof has taken place. In connection with the latter method, which is currently preferred, it is to be noted that, as sample begins to flow past the active zone adjacent layer 20 the refractive index does not start to change immediately due to the antibody/antigen reaction. There is thus sufficient time to take an initial reading with the unreacted sample flowing past, which reading can be utilised, using feedback circuitry to rapidly adjust the angle of incidence to an appropriate value half way down the reflectance dip so that the rest of the

test can be performed at this fixed angle.

In an embodiment of the invention, the hemisphere 11 is replaced by a hemicylinder. In this case Figures 3 and 4 can be regarded as sections through a suitable apparatus, with the hemicylinder 11 extending above and below the paper. The use of a hemicylinder gives the possibility of a line area of resonance instead of the single point 15, and hence a linear active zone. The aperture 24 becomes a slit, and the well 25 becomes elongate. The light source is operable to generate a "sheet" output beam which may be focussed by a cylindrical lens 3 onto line 15. The detector 18 is likewise linear in extent and is preferably composed of separate detectors or detector arrays, each arranged to monitor a specific section along the length of the line 15.

The hemicylindrical lens 11 has the advantage that it can be used to perform several tests simultaneously on a single sample. To this end, the layer 20 takes the form of a series of distinct sensitive areas, each comprising a different antibody, with each separate area being monitored by its own detector 18. A single sample introduced into well 25 will flow through the slot 24 into the active area and will react simultaneously with the various sensitive areas, giving individual output readings which can be monitored as detectors 18.

Although the hemisphere/hemicylinder 11 is shown as having a complete 180° curvature, in fact it will be noted that only that part near the flat surface is used and therefore a substantial portion of the body 11 can be cut away to form a truncated hemisphere or hemicylinder, as indicated, by way of example, by the dotted line 26 in Figure 4.

As will be appreciated from the foregoing, the invention enables a whole, or at least a significant part of, the spread of angles of interest to be investigated at once; the speed of investigation being limited only by the response characteristics of the detectors in the array 18 and of the associated sampling and computing circuits. This enables initial transients and other shifts which may occur during the analysis to be monitored and allowed for and also permits rapid calibratory checks to be made. Furthermore it has been found that, if each analysis, or assay, is started at a fixed value of reflectivity (as determined by a suitable output from the computing circuits) then the absolute refractive index of the fluid sample, which may well vary between samples, is unimportant. Importantly, the invention enables the desired reflectivity characteristic to be determined on a time scale so short that it is less than the time taken for the chemical bonding, necessary to SPR, to be achieved between the relevant constituent of the fluid sample and the reflective layer.

A further advantage of the invention is that it permits calibratory scans to be conducted with fluids of known SPR characteristics to generate compensating data which can be held in the computing circuits, and automatically applied as corrections if desired during clinical analysis. This compensating data can be used, for example, to allow for variations in reflectivity over the point 15, a phenomenon which can occur particularly if the reflective layer is produced by evaporation.

Figure 5 shows a representation of a video signal derived from the detector 18 in the arrangement of Figures 3 and 4, as displayed on an oscilloscope screen. The SPR resonance can be clearly seen.

The detector is electronically scanned, typically at approximately 200 times per second, to allow the movement of the resonance to be viewed in "real-time" as biochemicals are bound to the surface of the metal coated plate 16. The reflectivity curve in Figure 5a has been modulated by the approximately Gaussian profile of the beam from the laser diode source. This profile can be removed by appropriate signal processing as shown in Figure 5b, which was produced by subtraction of the fixed background due to ambient light and division by the signal without any resonance.

Claims

1. A sensor for use in biological, biochemical or chemical testing, said sensor comprising a block (11,16) of material transparent to electromagnetic radiation, a layer (19) of metallic material applied to at least part of a first surface (27) of said block, a layer (20) of sensitive material applied to the metallic layer, means for introducing onto the sensitive layer (20) so as to react therewith a sample to be analysed, a source of electromagnetic radiation (13), said radiation (13) being directed into said transparent block (11,16) in such a way as to be internally reflected off said part of said surface, and detector means positioned to receive the internally reflected beam, said sensor being characterised by means (14) for focussing said radiation onto said part (15) of said first surface (27) in such a way that the incoming beam is a converging fan beam that spans a range of angles of incidence including that which causes surface plasmon resonance to occur and that said incoming beam gives a point or line of incidence on said first surface, the characteristics of which resonance is dependent upon the reaction between the sample and the sensitive layer (20), and wherein said detector means (18) is operable to receive a range of angles within the span of the diverging fan

beam (17) resulting from the internal reflection of said incoming fan beam, which received range of angles is sufficient to enable said characteristics of the surface plasmon resonance to be detected.

2. A sensor as claimed in Claim 1 wherein the radiation from said source enters the block (11,16) through a second, curved, surface.
3. A sensor as claimed in Claim 2 wherein the centre of curvature of said second surface lies on said first surface (27).
4. A sensor as claimed in either one of Claims 2 or 3 wherein said second surface is circular.
5. A sensor as claimed in any one of Claims 2, 3 or 4 wherein the input beam of electromagnetic radiation enters the block (11,16) in a direction orthogonal to the tangent to the surface at the point of entry.
6. A sensor as claimed in any one of the preceding claims wherein said detector means (18) is positioned externally of said block (11,16), and wherein the internally reflected beam (17) emerges from said block through a third surface of the block, said third surface being curved.
7. A sensor as claimed in Claim 6 wherein the centre of curvature of said third surface lies on said first surface (27).
8. A sensor as claimed in any one of Claims 2 to 7 wherein said transparent body (11,16) takes the form of a hemisphere whose flat surface is said first surface (27) and whose circular surface includes said second surface, and wherein said part of said first surface is positioned at the centre of the first surface.
9. A sensor as claimed in any one of Claims 2 to 7 wherein said transparent body (11,16) takes the form of a hemicylinder whose flat surface is said first surface (27) and whose curved surface includes said second surface and wherein said part of said first surface is positioned on the longitudinal central axis of said first surface.
10. A sensor as claimed in either one of Claims 8 or 9 wherein the top part of the curved surface of the body (11,16) is omitted to give a truncated hemisphere or hemicylinder.

11. A sensor as claimed in any one of the preceding claims wherein the detector means (18) takes the form of a large-area detector positioned to collect the whole emergent beam.

12. A sensor as claimed in any one of the preceding claims wherein the detector means (18) takes the form of an array of angularly spaced detectors positioned to collect the whole emergent beam.

13. A sensor as claimed in any one of the preceding claims wherein said sensitive layer (20) takes the form of an antibody layer to be reacted with a sample containing a corresponding antigen.

Patentansprüche

1. Ein Sensor zur Verwendung in biologischen, biochemischen oder chemischen Testverfahren, wobei dieser Sensor umfaßt einen Block (11, 16) aus einem Material, das gegenüber elektromagnetischer Strahlung durchlässig ist, eine Schicht (19) eines metallischen Materials, das auf wenigstens einen Teil einer ersten Oberfläche (27) dieses Blocks aufgebracht ist, eine Schicht (20) eines empfindlichen Materials, aufgebracht auf die metallische Schicht, Mittel zur Einbringung einer zu analysierenden Probe auf die empfindliche Schicht (20), um damit zu reagieren, eine Quelle einer elektromagnetischen Strahlung (13), wobei diese Strahlung (13) auf solche Weise in den transparenten Block (11, 16) gerichtet ist, um intern von diesem Teil der Oberfläche reflektiert zu werden, und Detektormittel, die positioniert sind, um den intern reflektierten Strahl zu empfangen, wobei der Sensor charakterisiert ist durch Mittel (14) zur Fokussierung der Strahlung auf den Teil (15) der Oberfläche (27) auf solche Weise, daß der eintretende Strahl ein konvergierender Fächerstrahl ist, der einen Einfallswinkelbereich überspannt, der den einschließt, der Oberflächen-Plasmon-Resonanz auftreten läßt, und dieser eintretende Strahl einen Einfallspunkt oder -linie auf der ersten Oberfläche ergibt, wobei die Charakteristika der Resonanz von der Reaktion zwischen der Probe und der empfindlichen Schicht (20) abhängen, und wobei die Detektormittel (18) dazu in der Lage sind, einen Bereich von Winkeln innerhalb der Spanne des divergierenden Fächerstrahls (17), der sich aus der internen Reflektion des eintretenden Fächerstrahls ergibt, zu empfangen, wobei der empfangene Bereich von Winkeln ausreichend ist, die Charakteristika der Oberflächen-Plasmon-Reso-

nanz empfangen zu lassen.

2. Ein Sensor wie in Anspruch 1 beansprucht, wobei die Strahlung aus der Quelle in den Block (11, 16) durch eine zweite gebogene Oberfläche eintritt. 5
3. Ein Sensor wie in Anspruch 2 beansprucht, wobei das Zentrum der Krümmung der zweiten Oberfläche auf der ersten Oberfläche (27) liegt. 10
4. Ein Sensor wie in einem der Ansprüche 2 oder 3 beansprucht, wobei die zweite Oberfläche kreisförmig ist. 15
5. Ein Sensor wie in einem der Ansprüche 2, 3 oder 4 beansprucht, wobei der Eintrittsstrahl elektromagnetischer Strahlung in den Block (11, 16) in einer Richtung senkrecht zu der Tangente an der Oberfläche des Eintrittspunktes eintritt. 20
6. Ein Sensor wie in einem der vorhergehenden Ansprüche beansprucht, wobei die Detektormittel (18) außerhalb des Blockes (11, 16) positioniert sind und wobei der intern reflektierte Strahl (17) aus dem Block durch eine dritte Oberfläche des Blockes austritt, wobei die dritte Oberfläche gebogen ist. 25
7. Ein Sensor wie in Anspruch 6 beansprucht, wobei das Zentrum der Krümmung der dritten Oberfläche auf der ersten Oberfläche (27) liegt. 30
8. Ein Sensor wie in einem der Ansprüche 2 bis 7 beansprucht, wobei der durchlässige Körper (11, 16) die Form einer Halbkugel annimmt, deren flache Oberfläche die erste Oberfläche (27) darstellt und dessen kreisrunde Oberfläche die zweite Oberfläche einschließt, und wobei der Teil der ersten Oberfläche im Zentrum der ersten Oberfläche gelegen ist. 35
9. Ein Sensor wie in einem der Ansprüche 2 bis 7 beansprucht, wobei der durchlässige Körper (11, 16) die Form eines Halbzylinders annimmt, dessen flache Oberfläche die erste Oberfläche (27) ist, und dessen gebogene Oberfläche die zweite Oberfläche beinhaltet, und wobei der Teil der ersten Oberfläche auf der zentralen Längsachse der ersten Oberfläche gelegen ist. 40
10. Ein Sensor wie in einem der Ansprüche 8 oder 9 beansprucht, wobei der obere Teil der gebogenen Oberfläche des Körpers (11, 16) wegge-

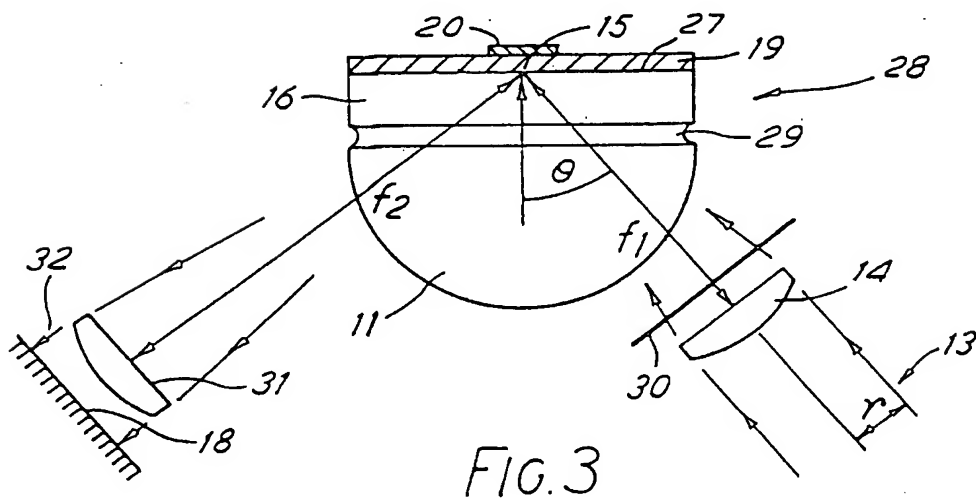
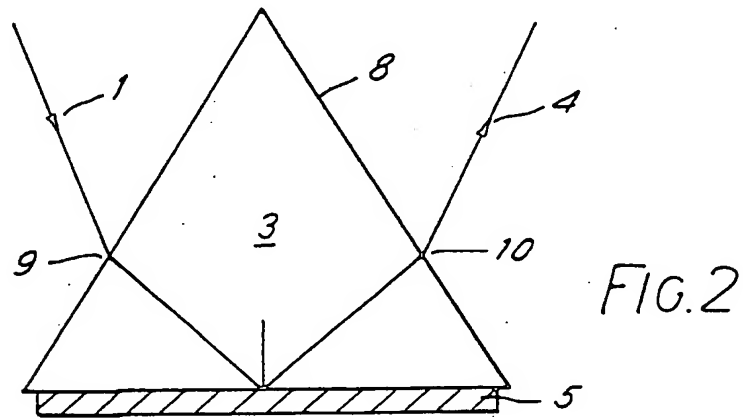
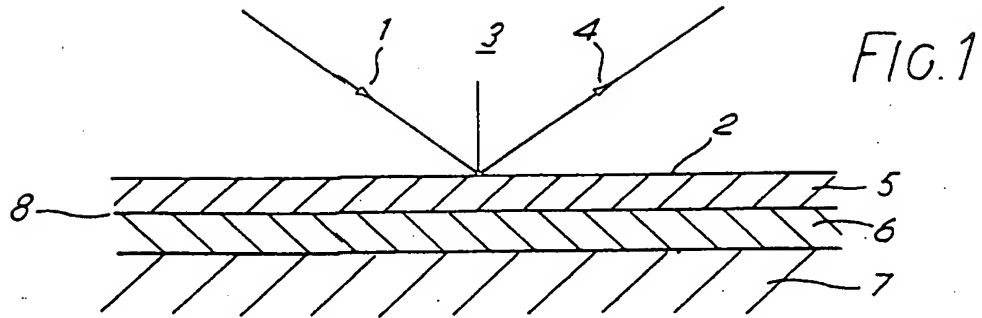
lassen ist, wobei sich eine abgestumpfte Halbkugel oder Halbzylinder ergibt.

11. Ein Sensor wie in einem der vorhergehenden Ansprüche beansprucht, wobei die Detektormittel (18) die Form eines groß-Flächen-Detektors einnehmen, der so positioniert ist, den gesamten austretenden Strahl zu sammeln. 45
12. Ein Sensor wie in einem der vorhergehenden Ansprüche beansprucht, wobei die Detektormittel (18) die Form einer Anordnung von in Winkeln beabstandeten Detektoren einnehmen, die angeordnet sind, den gesamten austretenden Strahl zu sammeln. 50
13. Ein Sensor wie in einem der vorhergehenden Ansprüche beansprucht, wobei die empfindliche Schicht (20) die Form einer Antikörperschicht einnimmt, die mit einer Probe, die einen entsprechenden Antikörper enthält, umgesetzt werden soll. 55

Revendications

1. Analyseur destiné à être utilisé dans des expérimentations biologiques, biochimiques ou chimiques, ledit analyseur comprenant un bloc (11, 16') de matière laissant passer la radiation électro-magnétique, une couche (19) de matière métallique étant déposée sur au moins une partie d'une première surface (27) dudit bloc, une couche (20) de matière sensible étant déposée sur la couche métallique, un moyen d'introduction d'un échantillon devant être analysé dans la couche sensible (20) de manière qu'il réagisse avec elle, une source de radiation électro-magnétique (13), ladite radiation (13) étant dirigée sur ledit bloc (11, 16) qui la laisse passer, de manière qu'elle subisse une réflexion interne et qu'elle sorte de ladite partie de ladite surface et un détecteur positionné de manière qu'il réceptionne le faisceau réfléchi intérieurement, ledit analyseur étant caractérisé par un moyen (14) de focalisation de ladite radiation sur ladite partie (15) de ladite première surface (27) d'une manière telle que le faisceau entrant soit un faisceau convergent en éventail qui couvre une plage d'angles d'incidence qui inclut celui qui fait apparaître la résonnance de plasmons superficiels et ledit faisceau entrant donnant un point ou une ligne d'incidence sur ladite première surface, les caractéristiques de ladite résonnance étant fonction de la réaction entre l'échantillon et la couche sensible (20) et en ce que ledit détecteur (18) est agencé pour réceptionner une plage d'angles située à l'intérieur de la largeur

- du faisceau divergent en éventail (17) qui résulte de la réflexion interne dudit faisceau entrant en éventail, ladite plage réceptionnée d'angles étant suffisante à permettre de détecter ladite caractéristique de la résonnance de plasmons superficiels.
2. Analyseur selon la revendication 1, dans lequel la radiation provenant de ladite source entre dans le bloc (11, 16) par une seconde surface qui est courbe.
3. Analyseur selon la revendication 2, dans lequel le centre de courbure de ladite seconde surface est situé sur ladite première surface (27).
4. Analyseur selon une ou l'autre des revendications 2 et 3, dans lequel ladite seconde surface est circulaire.
5. Analyseur selon l'une quelconque des revendications 2, 3 ou 4, dans lequel le faisceau d'entrée de la radiation électro-magnétique entre dans le bloc (11, 16) dans une direction perpendiculaire à la tangente à la surface au point d'entrée.
6. Analyseur selon l'une quelconque des revendications précédentes, dans lequel ledit détecteur (18) est placé à l'extérieur dudit bloc (11, 16) et dans lequel le faisceau réfléchi intérieurement (17) émerge dudit bloc par une troisième surface dudit bloc, ladite troisième surface étant courbe.
7. Analyseur selon la revendication 6, dans lequel le centre de courbure de ladite troisième surface est situé sur ladite première surface (27).
8. Analyseur selon l'une quelconque des revendications 2 à 7, dans lequel ledit corps transparent (11, 16) a la forme d'une hémisphère dont la surface plane est ladite première surface (27) et dont la surface circulaire comprend ladite seconde surface et dans lequel ladite partie de ladite première surface est placée au centre de la première surface.
9. Analyseur selon l'une quelconque des revendications 2 à 7 dans lequel ledit corps laissant passer la radiation (11, 16) a la forme d'un semi-cylindre dont la surface plane est ladite première surface (27) et dont la surface courbe comprend ladite seconde surface et dans lequel ladite partie de ladite première surface est placée sur l'axe de symétrie longitudinal de ladite première surface.
10. Analyseur selon l'une ou l'autre des revendications 8 ou 9, dans lequel la partie du sommet de la surface courbe du corps (11, 16) est supprimée de manière que ce corps constitue une hémisphère ou un semi-cylindre tronqué.
11. Analyseur selon l'une quelconque des revendications précédentes, dans lequel ledit détecteur (18) a la forme d'un détecteur de grande surface positionné de manière à recueillir la totalité du faisceau émergeant.
12. Analyseur selon l'une quelconque des revendications précédentes, dans lequel le détecteur (18) a la forme d'une série de détecteurs angulairement distants et placés de manière à recueillir la totalité du faisceau émergeant.
13. Analyseur selon l'une quelconque des revendications précédentes, dans lequel ladite couche sensible (20) a la forme d'une couche d'anticorps destinée à réagir avec un échantillon contenant un antigène correspondant.



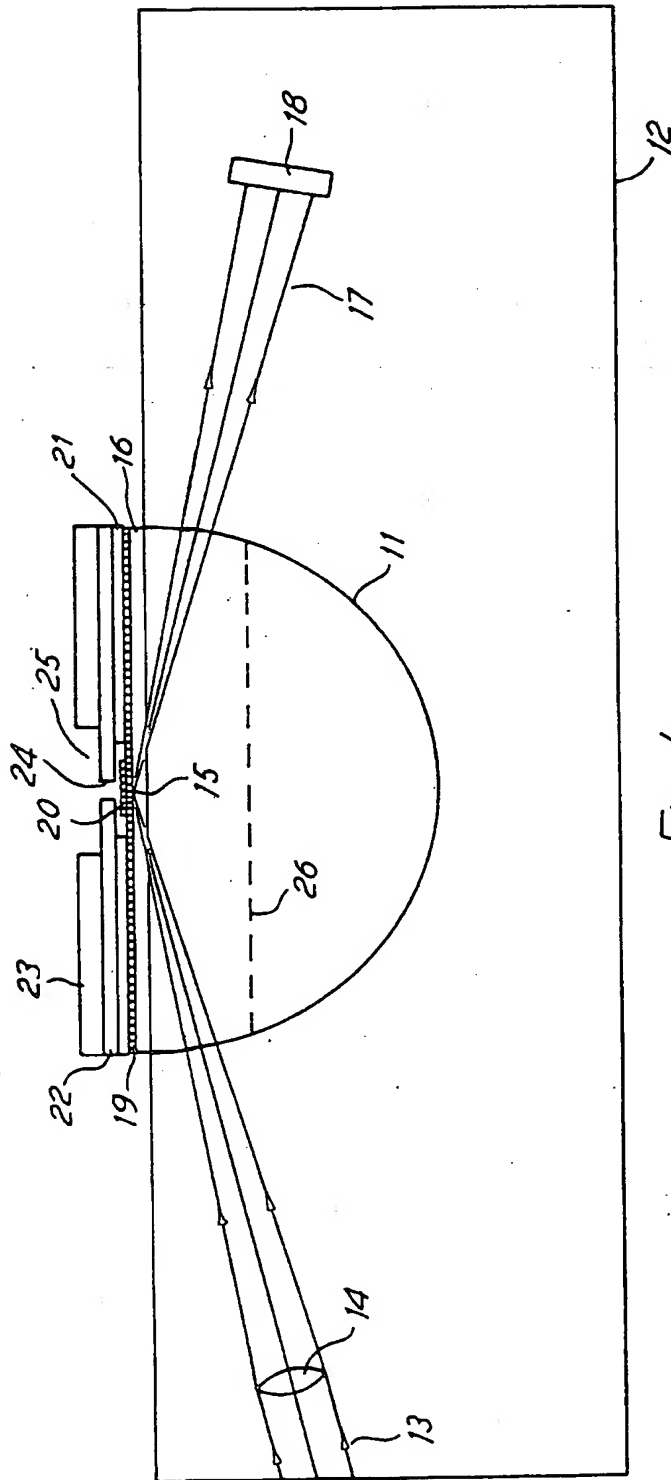


FIG. 4

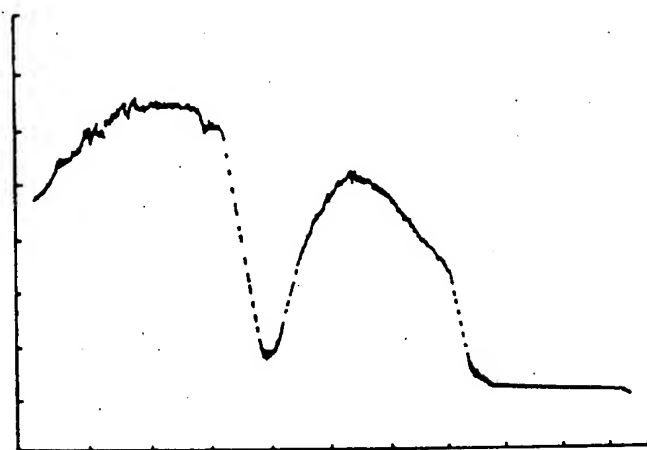


FIG.5(a)

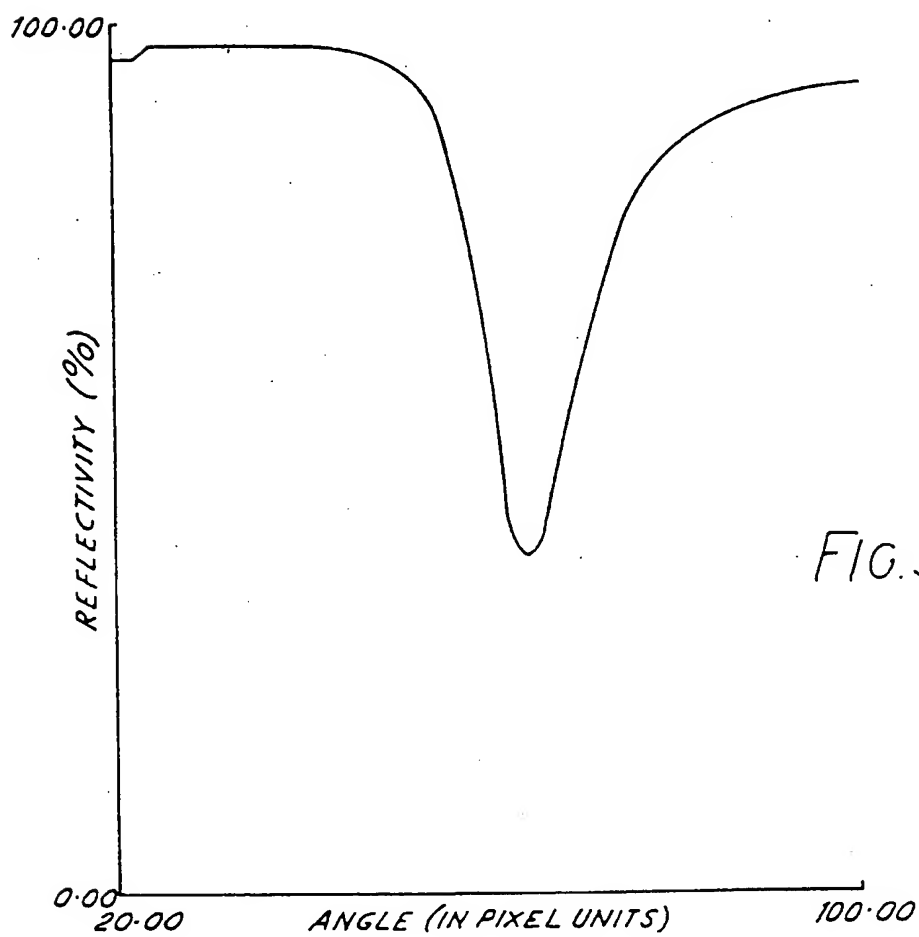


FIG.5(b)